# Medical Imaging Detectors for Real-Time Micro-Radiography

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## **1. Introduction**

Radiographic unsharpness results from geometric and detector unsharpness. Geometric unsharpness is affected by the size of the X-ray source in combination with source-to-object and object-to-detector distances. In conventional medical X-ray imaging using an X-ray tube, the highest spatial resolution is around 30  $\mu$ m. However, this is attained by mammography that produces a single high-resolution radiograph using an intensifying screen and film combination.

On the contrary, micro-radiography with a resolution higher than 30  $\mu$ m can be carried out using highresolution detectors and a nearly parallel X-ray beam provided by a third generation synchrotron radiation source at SPring-8. In SR radiography, the long source-to-object distance and the small source size overcome geometric unsharpness.

A micro-radiography system has been investigated as a diagnostic tool for circulatory disorders and early stage malignant tumors. Digital micro-radiography with 10  $\mu$ m resolution has been carried out at SPring-8 using two types of detectors designed for X-ray indirect and direct detection [1].

The indirect-sensing detector is a fluorescent-screen optical-lens coupling system using a high-sensitivity pickup-tube camera. A scintillator converts X-ray photons to visible light that is detected by the photoconductive layer of the pickup tube.

The direct-sensing detector consists of an X-ray direct-sensing pickup tube with a beryllium faceplate for X-ray incidence to the photoconductive layer. Absorbed X-rays in the photoconductive layer are directly converted to photoelectrons and signal charges are readout by electron beam scanning.

#### 2. Indirect-sensing Detector

In Fig. 1, X-rays passing through an aluminum window are transformed into a visible image on a fluorescent screen. The screen is made from gadolinium oxysulfide ( $Gd_2O_2S$ :Tb) phosphor. The phosphor layer is about 20 µm in thickness. A mirror deflects the luminescent light 90° to a high numerical aperture lens system that focuses it on a video camera [2]. Light paths are folded with the mirror to protect the lenses and the camera from direct X-ray impact.

The image sensing device used is a high-sensitivity pickup-tube, HARPICON. The pickup tube consists of an amorphous selenium photoconductive target and is characterized by its internal amplification system which uses stable avalanche multiplication of photogenerated carriers under a strong electric field in the photoconductive layer [3]. The HARPICON tube is 64 times more sensitive than conventional tubes.

The input field of  $20 \times 20$  mm on the screen is focused on a  $10 \times 10$  mm photoconductive layer by the high numerical aperture lens system. The limiting resolution is 20 µm when the images are stored in  $1024 \times 1024$  pixel digital format. The maximum speed of imaging is 30 images/sec in the 1050 scanning-line mode of the camera. The images are stored in a frame memory in 10-bit resolution.

The advantage of the indirect-sensing detector is that the fluorescent screen and lens can be changed quite easily. There are a few restrictions on the design of the input field size by adjusting the lens with an optimized demagnification factor under the condition of X-ray quantum-noise-limited imaging [4].



Fig. 1. View of X-ray indirect-sensing detector.



Fig. 2. View of X-ray direct-sensing detector.

## 3. Direct-sensing Detector

An X-ray direct-sensing vidicon-type pickup-tube camera was developed in the 1960's with a PbO photoconductive layer for the observation of real-time topography images combined with a high power X-ray generator. After that, the resolution of the directsensing pickup tube was improved. The X-ray SATICON tube with an amorphous photoconductive Se-As alloy target was developed for the use of synchrotron radiation experiments of live topography at the Photon Factory in Tsukuba [5].

The direct-sensing camera was further improved with the introduction of high-definition television (HDTV) which increases resolution to 1050 scanning lines. The new X-ray SATICON camera in Fig. 2 has the same resolution of 1050 scanning lines at present. However, the camera has been designed to improve its resolution to 2100 scanning lines.

The X-ray pickup tube was developed for higher resolution real-time imaging than the indirect-sensing detector using fluorescent-screen optical-lens coupling. The light scatter on the fluorescent screen is the dominant loss of resolution and this process is not present in the X-ray pickup tube. Charge carriers move in a path parallel to an electric field without deflection in the photoconductive layer. The spatial resolution of the direct-sensing tube depends only on the diameter of the scanning electron beam.

The new camera can take images at a speed of 30 images/sec. The digital images are acquired after analog-to-digital conversion synchronizing the timing with the electron beam scanning in the pickup tube. High-resolution images are stored in digital frame memory in 10-bit resolution at the maximum speed of imaging.

However, the disadvantage of the direct-sensing detector is that it does not have an iris. X-ray incident flux to the pickup tube should be adjusted to obtain an optimized output signal level from the camera.

#### **4. Resolution of Detector**

The performance of the direct-sensing pickup-tube camera was evaluated at the medium length bendingmagnet beamline SPring-8 BL20B2 by taking an image of a spatial resolution chart. Images were obtained in the 1050 scanning-line mode of the camera at an input field size of  $10 \times 10$  mm. Figure 3 displays a whole chart image in  $1024 \times 1024$  pixel digital format. Figure 4 shows a digital zoomed image of the central portion in Fig. 3. The numerical values in Fig. 4 show the width of the stripes.

The limiting spatial resolution is about 10  $\mu$ m equal to the pixel size on the photoconductive layer. By using this detector, small blood vessels with diameters of 20-30  $\mu$ m can be visualized. The resolution will improve to 5  $\mu$ m with a camera operated at a 2100 scanning-line mode. The image will be stored at a speed of 7.5 images/sec in 2048×2048 pixel digital format.



Fig. 3. Whole image of resolution chart.



Fig. 4. Digital zoomed image of resolution chart.

#### References

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